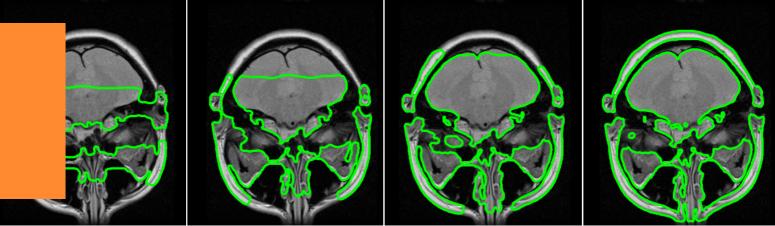


## Medical Imaging

Segmentation with Level Sets



Contour propagation by initial conditions (40, 100, 150 and 200 iterations)

Segmentation (i.e. delineation of anatomical structures in image data) plays a crucial role in medical imaging. Due to the complexity and variability of anatomic shapes segmentation is still a big challenge.

A wide variety of segmentation techniques have been proposed: a) traditional low-level image processing techniques [1] which consider only local information and generates infeasible object boundaries and b) more robust techniques with deformable models [2] which exploits constraints from the image data (bottom-up) together with "a priori" knowledge about the shape (topdown).

The Institute for Medical and Analytical Technologies is focusing in the field of Medical Imaging on Data-Visualization, -Analysis and Modeling. The study of segmentation tech-niques is therefore a fundamental issue.

For efficient and robust segmentation of various anatomic structures we implemented the Chan-Vese- algorithm (a deformable model with Level Sets).

## Algorithm

The Chan-Vese algorithm is an deformable model approach with contour evolution based on the Mumford-Shah functional, and the level sets of Osher and Sethian. A comprehensive description is given in [3].

$$E[C] := \lambda_{in} \cdot \int_{\Omega_{in}} (I(x) - c_{in})^2 + \lambda_{out} \cdot \int_{\Omega_{out}} (I(x) - c_{out})^2 + \gamma \cdot L_C$$

Given a gray-value image  $I(x) : \Omega \to R^+$ , the Chan- Vase algorithm minimizes the energy to define the contour *C* that partitions the image domain  $\Omega$  into two subdomains  $\Omega_{in}$ ,  $\Omega_{out}$  (where  $C_{in}$ ,  $C_{out}$  are the average gray-values in the sub-domains,  $L_C$  is the length of the contour *C* and  $\lambda_{in}$ ,  $\lambda_{out}$ ,  $\gamma$  are design parameters).

The propagation of C (on  $R^2$ ) is solved by using Euler-Lagrange (PDE on  $R^2$ ) and approxi-mation (Interation).

## **Results Conclusion**

First applications with specific anatomical structures (brain, vessels, spine) led to robust and accurate segmentation results. And a strength of the algorithm is its ability to handle the topology changes (level sets).

Due to the inability to distinguish between different shapes (no model-information) the algorithm is mainly useful for semi-automated segmentation.

## References:

[1] Bezdek, J.C., et .al.:Review of MR image segmentation techniques unsing pattern recognition. Med.Phys., vol. 20, no4, 1993.

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[3] T. Chan and L. Vese. An active contour model without edges. Int. Conf. Scale-Space Theories in Computer Vision, 16(2):266-277, 1999.

We invite you to explore and develop new ideas together with us!

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